

In vitro inhalation bioaccessibility of phthalate esters and alternative plasticisers present in indoor dust using artificial lung fluids

Article

Accepted Version

Kademoglou, K., Giovanoulis, G., Palm-Cousins, A., Padilla-Sanchez, J. A., Magnér, J., de Wit, C. A. and Collins, C. D. (2018) In vitro inhalation bioaccessibility of phthalate esters and alternative plasticisers present in indoor dust using artificial lung fluids. Environmental Science and Technology Letters, 5 (6). pp. 329-334. ISSN 2328-8930 doi: 10.1021/acs.estlett.8b00113 Available at https://centaur.reading.ac.uk/82313/

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To link to this article DOI: http://dx.doi.org/10.1021/acs.estlett.8b00113

Publisher: American Chemical Society

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1 Graphical abstract



3 Highlights

4	•	First study on <i>in vitro</i> inhalation bioaccessibility of organics from house dust
5	•	Gamble's solution and artificial lung fluid were used as pulmonary surrogate media
6	•	DMP and DEP were > 75 % bioaccessible in both lung media
7	•	Alterative plasticisers DINCH and DEHT were < 5% bioaccessible
8	•	Inhalation bioaccessibility was highly influenced by hydrophobicity
9		

- 10 In vitro inhalation bioaccessibility of phthalate esters and alternative plasticisers present in
- 11 indoor dust using artificial lung fluids
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25

26 Abstract

27 Phthalate esters (PEs) are plasticiser additives imparting durability, elasticity and flexibility 28 to consumer products. The low migration stability of PEs along with their ubiquitous 29 character and adverse health effects to humans and especially children has resulted in their 30 classification as major indoor contaminants. This study assesses inhalation exposure to PEs 31 via indoor dust using an *in vitro* inhalation bioaccessibility test (*i.e.* uptake) for of dimethyl 32 phthalate (DMP), diethyl phthalate (DEP) and di-(2-ethylhexyl) phthalate (DEHP) and the 33 alternative non phthalate plasticisers bis(2-ethylhexyl) terephthalate (DEHT) and 34 cyclohexane-1,2-dicarboxylic acid diisononyl ester (DINCH), exposure. Using artificial lung 35 fluids, which mimicktwo distinctively different pulmonary environments, namely artificial 36 lysosomal fluid (ALF, pH = 4.5) representing the fluid that inhaled particles would contact 37 after phagocytosis by alveolar and interstitial macrophages within the lung and Gamble's 38 solution (pH = 7.4), the fluid for deep dust deposition within the pulmonary environment. Low molecular weight (MW) PEs such as DMP and DEP were highly bioaccessible (> 75 %) 39 40 in both artificial pulmonary media, whereas highly hydrophobic compounds such as DEHP, DINCH and DEHT were < 5 % bioaccessible via the lung. Our findings show that the *in vitro* 41 42 pulmonary uptake of PEs is primarily governed by their hydrophobicity and water solubility, 43 highlighting thus the need for the establishment of a unified and biologically relevant 44 inhalation bioaccessibility test format, employed within the risk assessment framework for 45 volatile and semi-volatile organic pollutants. 46

Keywords: bioaccessibility, inhalation, phthalate esters, indoor dust, artificial lysosomalfluid, DINCH

49

50 Introduction

51 Phthalate esters (PEs) are plasticiser additives enhancing durability, elasticity and flexibility

52 in consumer and polymeric products ¹. Low molecular weight (LMW) PEs such as dimethyl

53 phthalate (DMP) and diethyl phthalate (DEP) are added as synthetic stabilisers to industrial

54 solvents and personal care products they are also used as colouring or fragrance additives ^{2,3}.

55 High MW (HMW) PEs such as di-(2-ethylhexyl) phthalate (DEHP) and di-iso-nonyl

56 phthalate (DiNP) are primarily used in polyvinyl chloride (PVC) products including floor

57 polishing, wall coatings, children's toys, medical products and food packaging ^{4–6}. Their low

58 migration stability and vapour pressure influence PE release to the indoor environment,

resulting in their classification as major indoor organic contaminants ^{7,8}. Consequently,

60 considerably high levels of PEs have been found in indoor dust worldwide 5,9-13.

61 Human exposure to PEs in the indoor environment is a phenomenon of growing concern due

62 to the potentially adverse health effects of PEs such as DEHP, di-n-butyl phthalate (DnBP)

and di-iso-butyl phthalate (DiBP) in adults, such as disrupted endocrine and thyroid

64 homeostasis, reduced fertility and reproduction ^{3,14,15}. Hence, the US and the EU have partly

restricted the use of DiBP, DnBP, and DEHP in toys and childcare products ^{16,17}. Such

66 actions paved the way for the introduction of less toxic, non-phthalate substitutes (*i.e.*

alternative plasticisers) in consumer products in the early 2000s, such as di-isononyl-

68 cyclohexane-1,2-dicarboxylate (DINCH; DEHP and DiNP replacement) and bis(2-

69 ethylhexyl) terephthalate (DEHT), a structural isomer of DEHP^{18–21}. However, due to their

70 dominant use and rapid substitution, considerable levels of DINCH and DEHT have been

reported in the indoor environment, raising concerns about their potential effects on humans 22-25.

73 Due to their critical and vulnerable developmental status, pre and postnatal children's 74 exposure to PEs via indoor dust and PVC materials has been linked with chronic respiratory problems such as allergies, asthma, bronchial hyperactivity and inflammation, as well as 75 neurodevelopmental disorders manifesting in adulthood ^{26–31}. Franken et al. (2017) reported 76 77 the high occurrence of asthma in Belgian teenagers (especially girls) associated with high DEHP and DnBP exposure ³². DEHT and DINCH administration to rodents revealed no signs 78 of DEHP-like toxicity ^{33–35}. However, DINCH in utero exposure has been associated with 79 80 signs of impaired liver metabolism and premature testicular aging such as decreased 81 testosterone secretion, physical changes in seminal glands and testicular atrophy in rats and

- their young offspring ³⁶. Thus, the debate regarding the safety of alternative plasticisers is
 ongoing especially during early-life exposure.
- 84 Physiologically-based extraction tests (PBET) have been employed to assess the oral
- 85 bioaccessibility (*i.e.* uptake) of PEs via dust ingestion ^{37–39}. PE gut bioaccessibility decreased
- as logK_{ow} increased; LMW PEs such as DMP and DEP were found to be 32 % and 26 %
- bioaccessible, respectively, while DEHP was only 10 % bioaccessible via the gut ³⁸. In a
- 88 comparative study between different dust size fractions and oral bioaccessibility, Wang et al.
- 89 (2013) reported the highest gut uptake for LMW PEs in $< 63 \mu m$ size fraction, compared to
- 90 particles > 63 μ m³⁹. Dermal absorption of DEP and DnBP directly from air has been
- 91 proposed by Weschler et al⁴⁰. Since no studies exist regarding the inhalation bioaccessibility
- 92 of organic pollutants, this calls for their development 41 .

93 This is the first study we are aware of quantifying the inhalation bioaccessibility of PEs and

94 alternative plasticisers employing two artificial lung fluids, mimicking two distinctively

- 95 different interstitial lung conditions. Artificial pulmonary fluids have been previously
- 96 employed in inhalation bioaccessibility studies of water-soluble metals and nanoparticles ^{42–}
- 97 ⁴⁶. Artificial lysosomal fluid (ALF, pH=4.5) represents the fluid which inhaled particles come
- 98 into contact with after phagocytosis by alveolar and interstitial macrophages within the lung.
- 99 Gamble's solution (GMB, pH=7.4) is a surrogate fluid for deep dust deposition within the
- 100 interstitial fluid of the lung 43,46 . The objectives of the present study are to evaluate the *in*
- 101 vitro inhalation bioaccessibility of PEs, DINCH and DEHT present in indoor dust by
- 102 employing two different artificial pulmonary fluids, *i.e.* Gamble's solution and ALF
- 103 representing the healthy and inflammatory status of the tracheobronchial environment,
- 104 respectively and to assess possible factors influencing inhalation bioaccessibility of PEs,
- 105 DINCH and DEHT.

Material and methods

- 107 Sampling and dust particle properties
- 108 Details on the A-TEAM sampling protocols are given elsewhere⁴⁷. Pre-existing vacuum
- 109 cleaner dust samples (N=10) were passed through a methanol-washed, metallic sieve (< 63
- 110 μm) with respect to the inhalable aerodynamic particle cut off convention according to the
- 111 International Organization for Standardization (ISO)⁴⁸. Specific surface area and dust particle
- size were determined by laser diffraction spectroscopy (Mastersizer 3000, Malvern Ltd.,

113 UK), while total carbon (TC %) and nitrogen (TN %) contents were determined by Thermo

- 114 Flash 2000 and organic matter content (OMC %) was determined by loss-on-ignition (LOI)
- 115 as described elsewhere 49 .

116 Dust extraction and clean-up

117 Details of the indoor dust extraction have been published previously ^{24,50}. Briefly, 100 mg of

118 dust (< 63 µm) were extracted with 10 mL acetone: n-hexane (1:1 v/v) using microwave-

assisted extraction (MAE) under controlled pressure and temperature. Prior to extraction, 400

120 ng ISTD mix prepared in n-hexane (DMP-d₄, DnBP-d₄ and DEHP-d₄) were spiked into all

121 samples. The dust extracts were concentrated to 0.5 ml under a gentle nitrogen (N₂) stream

122 which was filtrated through a glass Pasteur pipette tip containing charcoal in order to

123 eliminate any traces of external contamination and the solvent was exchanged to n-hexane.

124 This solution was loaded onto an ENVI-Florisil cartridge (500 mg / 3 mL, Biotage Isolute,

125 Uppsala, Sweden) and 9 mL of n-hexane were added as a cleaning elution step. During the

second elution, all target analytes were eluted using the 9 mL acetone: n-hexane (1:1) and the

resulting eluate was concentrated to 1 ml with a gentle N₂ flow at room temperature, filtered

- 128 as described above. Finally, all extracts were transferred to GC vials and biphenyl (300 ng)
- 129 was added as an injection recovery standard prior to GC-MS/MS analysis (Fig SI 1). Further

130 details about instrumental analysis are available in SI.

131 Lung fluid extraction

132 All lung fluid extractions were conducted in duplicate. Both media were freshly prepared 24

133 h before the initiation of each test in ultra-pure H₂O (18.2 Ω) as described elsewhere⁴³ (Table

134 SI 3), pH-adjusted using HCl 1 M and NaOH 1 M, stored at 4°C and were checked for

135 background phthalate contamination prior use. According to Boisa et al (2014), the

136 experimental volume for simulated lung fluid extraction tests should be equal to 20 mL,

137 given the pulmonary fluid volume capacity of healthy non-smoking adults (0.3 mL / kg; 70

138 kg body mass)⁴². In order to maintain 1:100 solid-to-liquid (S/L) ratio between the incubated

matrix and the pulmonary fluid, 0.2 g of indoor dust (< $63 \mu m$) were combined with 20 mL of

140 each artificial lung fluid separately, as suggested by Schaider et al⁵¹. All samples were

- 141 covered on top with oven-baked aluminium foil to avoid background phthalate
- 142 contamination, followed by continuous incubation inside a thermostatic chamber (60 rpm; 37
- [°]C) for 96 h, a time point relevant to the human alveolar clearance capacity ^{45,52}. After 96 h,
- 144 the samples were separated by centrifugation (1500 rpm; 3 min) and the lung supernatants

145 were subjected to liquid-liquid extraction (LLE) using 7 mL Hexane: MTBE 3:1 twice, while ultrasonication-assisted extraction was employed for the residual dusts twice for 10 min using 146 147 7 mL of Acetone: Hexane 1:1. Prior to all extractions, all samples were spiked with 400 ng 148 ISTD mix prepared in n-hexane (DMP-d₄, DnBP-d₄ and DEHP-d₄). To avoid any water 149 residue and remove any gel-like emulsion formulated during LLE, sufficient amount of oven-150 baked Na₂SO₄ (powder) was added to all extracts, followed by 1 min vortexing and organic 151 phase collection after centrifugation (1500 rpm; 3 min). All extracts were combined, solvent 152 was exchanged to n-hexane and concentrated to 1 ml under a gentle N2 stream at room 153 temperature, filtered as described above. The residual dust extracts were subjected for clean-154 up through ENVI-Florisil SPE cartridge (500 mg / 3 mL, Biotage Isolute, Uppsala, Sweden), similarly to the dust extraction procedure described above. Briefly, the residual dust extracts 155 were loaded onto the Florisil[®] columns, the first hexane eluate was discarded, while the 156 157 second eluate was collected using 9 mL of MTBE. The resulting eluate was concentrated to 1 158 ml under a gentle N₂ flow at room temperature, filtered as described above. Finally, all 159 extracts were transferred to oven-baked GC vials and biphenyl (300 ng) was added as an 160 injection recovery standard prior to GC-MS/MS analysis (Fig SI 2).

161 Data analysis

Inhalation bioaccessibility (IBAF) was determined using Eq. 1, where mass phthalate (lung supernatant) is set as the phthalate mass (ng) determined in the lung supernatant of the *in vitro* pulmonary system and mass phthalate (dust residual) is the mass (ng) determined in the dust residual collected after the 96 h-incubation of the *in vitro* pulmonary system which is considered as the non-bioaccessible fraction.

168 IBAF%

$$169 = \frac{mass phthalate (lung supernatant)}{mass phthalate (lung supernatant) + mass phthalate (dust residual)} x 100 (Eq. 1)$$

$$167$$

$$170 \quad \text{GraphPad Prism}^{\textcircled{\text{0}}} \text{ version 7.00 for Windows, (GraphPad Software, La Jolla CA, USA) was used for statistical analysis. Prior to statistical analysis, all data were checked for normality using the Shapiro–Wilk test and not all data passed the normality test. All data were arc-sine transformed, as this mathematical transformation is necessary for statistical analysis of results set in percentages in order to equalise variances among treatments 53. Ordinary two-way ANOVA (Uncorrected Fisher's test, p<0.05) was performed to assess statistically significant$$

- 176 differences of target analytes between both pulmonary fluids. Spearman's correlation
- 177 (p<0.05) was employed to assess statistical dependence and correlation between artificial
- 178 lung fluids and the physicochemical properties of all target analytes.
- 179 Quality assurance and quality control
- 180 The methods were evaluated using SRM 2585 as QC sample during dust (n=5) and lung fluid
- 181 (n=4) extractions, respectively. Oven-baked, uncontaminated sand was used as a procedural
- 182 blank during dust extractions; four blank lung fluid samples with no added matrix (two for
- 183 each lung fluid) were sequentially incubated and analysed as procedural blanks. The results
- 184 were blank-corrected for all target analytes by subtraction of the mean blank values from the
- 185 raw target analytes values (expressed in ng g^{-1}) according to Abdhalah and Covaci⁵⁴.
- 186 Extraction efficiency for all target analytes ranged from 70 120% for both lung fluids
- 187 respectively (Table SI 6). Method limits of detection (mLOD) were calculated as three times
- 188 the standard deviation of the lung fluid blanks (Table SI 7).

189 Results and discussion

- 190 PEs and alternative plasticisers in indoor dust
- 191 Apart from DEHT, levels of PEs and DINCH from floor (N=61) and vacuum cleaner dust
- 192 (N=58) from the ATEAM cohort have been previously reported ²³ and were of the same order
- 193 of magnitude as reported here (N=10; SI Table xxx). Besides the smaller dust particle size
- used in this study compared to Giovanoulis et al.²³ (< 63 μ m and < 500 μ m, respectively), the
- 195 median values for all target analytes were marginally different apart from DINCH (this study:
- 196 17.06 μ g g⁻¹, Giovanoulis et al.: 32.82 μ g g⁻¹; p<0.05). Substantial differences between the
- 197 maximum values of two studies were also found, e.g. DEP (this study: $54.2 \ \mu g \ g^{-1}$,
- 198 Giovanoulis et al: 240 μ g g⁻¹) or DiNP (this study: 2470 μ g g⁻¹, Giovanoulis et al: 1490 μ g g⁻¹
- ¹). These findings can be attributed to a) differences in sample size assessed and b)
- 200 differences in particle size cut off and specific surface area which are likely to influence a
- 201 pollutant's concentration in dust ^{39,55}. However, the aim of the present study is primarily to
- 202 assess the inhalation bioacceessibility of PEs and their alternatives plasticisers, rather than
- 203 report on their levels in dust.

204 Inhalation bioaccessibility

205 This is the first study on the *in vitro* inhalation bioaccessibility of PEs and alternative

206 plasticisers via indoor dust. Inhalation bioaccessibility for DMP and DEP exceeded 70 % in

207 both pulmonary media (Fig. 1). Statistical comparison of IBAF between the two pulmonary

208 media did not reveal any statistically significant differences for any target analyte regarding

209 the fluids' pH (pH Gamble's = 7.4; pH ALF = 4.5) and composition, apart from DMP

210 (p=0.017) with 71 % and 82 % IBAF for Gamble's solution and ALF, respectively. DEP was

also readily absorbed with 76 % and 75 % IBAF in Gamble's solution and ALF, respectively

212 (p>0.05), showing thus that inhalation is an important route of exposure for LMW PEs.

213 Gamble's solution is representative of the interstitial fluid of the deep lung area and ALF is

214 representative of the more acidic environment following phagocytosis by alveolar and

215 interstitial macrophages within the lung ^{42,43}. Hence, the inhaled dust particles would not have

to be phagocytised before a considerable uptake of plasticisers occurs, with the exception of

217 DMP.

218 Similarly to gut bioaccessibility which is partly governed by a pollutant's physico-chemical

219 properties including MW and $\log K_{ow}$ ^{56,57}, inhalation bioaccessibility of PEs decreased

against the increasing trend in MW and log Kow (> 4). DiBP pulmonary uptake was 15.5 %

and 12 %, in Gamble's solution and ALF, respectively, whereas DnBP and HMW PEs were

222 10 % and < 5 % bioaccessible in both media, including DEHP and its alternatives, DEHT and

223 DINCH (Fig 1). Such findings endorse ingestion (food or dust) and dermal uptake as the

224 predominant exposure routes for medium and HMW PEs, strongly influenced by their

225 hydrophobic character and low water solubility ^{6,23,38}. However, no consensus exists

regarding pulmonary media composition for inhalation bioaccessibility studies of organics.

227 Employing modified media formulations with the addition of biologically relevant pulmonary

surfactants such as albumin, mucin and dipalmitoylphosphatidylcholine (DPCC) have been

proposed ^{41,42,58}; the case of DPCC makes biological sense and it should be thus

230 systematically investigated along with other test parameters including S/L, incubation

duration and particle size cut off ^{41,59}, aiming towards a unified approach similarly to gut

232 bioaccessibility⁵⁶.

233 Method performance using SRM 2585

234 Method performance was assessed using SRM 2585, since the pulmonary media used here

235 were initially designed for nanoparticle and trace element inhalation bioaccessibility

studies^{43,45,60}. IBAF > 75 % was found for LMW PEs, while DEHP and DiNP were the least
bioaccessible (IBAF < 5 %) as highly hydrophobic compounds (Table 1), following a
comparable pattern to the Norwegian house dust IBAF results. The SRM 2585 batch
purchased in our study was prepared using a pool of dust samples collected during mid to late
1990s. Thus, DINCH and DPHP were not detected, since they were introduced in the market

- 241 after 2000^{18,61}.
- 242 In this study we propose an *in vitro* method regarding the inhalation bioaccessibility of PEs
- and their alternatives via indoor dust. Low MW PEs such as DMP and DEP were highly
- bioaccessible in both artificial pulmonary media (> 75 %), regardless of the medium's pH
- and composition. Unlike DEP which presented similar pulmonary uptake in both media,
- 246 DMP was more readily absorbed through ALF than Gamble's solution. HMW PEs along with
- 247 DEHP alternatives, DEHT and DINCH did not exceed 5 % pulmonary uptake. Therefore,
- 248 inhalation is a considerable route of exposure for LMW and less hydrophobic PEs. The lung
- 249 uptake potential for compounds with comparable physico-chemical properties, *e.g.* LMW
- 250 polycyclic aromatic hydrocarbons (PAHs) or organophosphates (PFRs) should be further
- assessed. Our results show that inhalation bioaccessibility of organic pollutants is primarily
- 252 governed by hydrophobicity and water solubility. Future research should be targeted towards
- a unified and biologically relevant *in vitro* pulmonary uptake test for organics relevant to dust
 deposition in the lung, human lung function and inflammation *in vivo*. Finally, animal studies
 are more representative of the *in vivo* situation, marking them as necessary for the validation
 of *in vitro* inhalation bioaccessibility tests.

257 **Conflict of interest**

258 The authors declare no conflict of interest.

259 Acknowledgments

260 The research leading to these results has received funding from the European Union Seventh

- 261 Framework Programme FP7/2007–2013 under grant agreement n° 316665 (A-TEAM
- 262 project). Katerina Kademoglou and George Giovanoulis would like to thank Dr. Yolanda
- 263 Hedberg from KTH (Sweden) for her help and useful guidance during the experimental
- 264 design. We acknowledge Dr. Eleni Papadopoulou and Dr. Juan Antonio Padilla Sanchez from
- 265 NIPH (Norway) for their help during the ATEAM sampling campaign. The writing up of this

- 266 manuscript was supported by the National Sustainability Project of the Czech Ministry of
- 267 Education (project number here) and the RECETOX Research Infrastructure (LM2015051
- and CZ.02.1.01/0.0/0.0/16_013/0001761). Katerina Kademoglou would like to thank Dr.
- 269 Shovonal Roy (UoR) for his useful comments on the statistical analysis and acknowledge the
- 270 financial support from the Mediterranean Scientific Association of Environmental Protection
- 271 (MESAEP) during her PhD studies by means of the Emmanuel Lahaniatis award for young
- 272 scientists.



273 Artwork and tables

Figure 1 – *In vitro* inhalation bioaccessibility (IBAF%) of phthalate esters and alternative plasticisers present in indoor dust samples (N=10), using two different simulated lung fluids, namely Gamble's solution (GMB) and artificial lysosomal fluid (ALF). Statistically significant differences shown here (*; p<0.05). Bar charts represent average values in duplicates. Error bars represent 1 STDEV.

Table 1 - Lung fluid method performance using SRM 2585 (n=4) for Gamble's solution and

281 artificial lysosomal fluid (ALF)

Target analytes [†]	Gamble's IBAF% (n=2)	STDEV	ALF IBAF% (n=2)	STDEV
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DMP	89.9	1.8	89.5	0.3
DEP	80.7	1.2	73.7	1.0
DiBP	17.6	2.7	8.0	0.6
DnBP	9.8	1.3	6.2	0.5
BzBP	18.5	3.6	13.2	0.6
DEHP	3.1	1.6	2.0	0.2
DEHT	4.9	1.6	4.6	0.6
DiNP	3.9	1.0	3.5	0.3

- ^{*}DINCH and DPHP not present in SRM 2585
- 283 Table 2 Spearman's correlation between inhalation bioaccessibility (IBAF) in Gamble's
- solution (GMB) and artificial lysosomal fluid (ALF) and the physicochemical properties ofplasticisers studied here

	GMB IBAF		ALF IBAF	
Physico-chemical properties [†]	Spearman's p	p value	Spearman's p	p value
MW	-0.561	0.096	-0.561	0.096
Log Kow	-0.705	0.027*	-0.705	0.027*
Log Koa	-0.588	0.081	-0.624	0.060
Vapour pressure	-0.535	0.115	-0.559	0.098
Water solubility	0.661	0.044*	0.636	0.054

- 286 *levels of statistical significance: p<0.05
- 287 † Physicochemical properties of plasticisers studied here can be found at Table SI xxx

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